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(64) Transplantable artificial tissue and process.

(67) A transplantable artificial tissue matrix structure containing viable cells which is suitable for insertion into the body is made by polymerizing precursors in an aqueous solution to form a shape retaining solid matrix comprising viable cells, matrix polymer and reversible gel polymer. The solution contains a matrix polymer precursor, a reversible gel polymer precursor, and viable cells. The reversible gel polymer is dissolved and removed to yield an insoluble, porous matrix containing viable cells. The conditions and reagents are selected to maintain the viability of the cells. The invention is particularly suitable for artificial transplant matrix tissue containing pancreatic islet cells.

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TRANSPLANTABLE ARTIFICIAL TISSUE AND PROCESS

This invention relates to an artificial tissue composition for insertion into the body and to the process for preparing it. In particular, this invention relates
5 to a matrix composition containing cells which can be inserted to introduce the cells into the body and to the process of preparing this matrix. In one particular aspect, this invention relates to preparation of a matrix containing pancreatic B-cells which, when inserted into
10 the body, can function as an artificial pancreas, introducing insulin produced by the B-cells cells into the body as needed.

Insertion of a missing cell type into the body can be
15 accomplished by implantation, transplantation or injection of cells. The cells can be in the form of tissue fragments, clumps of cells or single cells derived from the fragmentation of organs or tissues. Alternatively, the cells can be clumps of cells or single cells derived
20 from cell culture, tissue culture or organ culture. If the cell insertion is to be successful, however, the cells must have the physiological environment after insertion required for the reorganization, growth or differentiation necessary to permit normal functioning in the body. The
25 cells inserted into the body must be maintained in a physical relationship which permits adaptation to the new environment and promotes the changes which are required before normal cell functioning can occur.

Diabetes mellitis is an example of a disease state
30 associated with an insufficiency or absence of certain types of cells in the body. In this disease, pancreatic B-cells are missing or deficient. The condition can be ameliorated by the successful insertion of the missing pancreatic B-cell.

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Prior to this invention, attempts to introduce such cells into the body have not achieved the natural reorganization, growth or differentiation needed for optimum cell functioning in the body.

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Prior art processes for inserting cells have been generally unsuccessful, primarily because they have not satisfied the cellular requirement of transplantation. Attempted matrix approaches have failed to form the matrix
10 rapidly and without cellular damage. They have failed to provide shape and size control, the cell density required for proliferation, the matrix porosities for diffusion of nutrients and macromolecules, or the environment effecting cell-to-cell contact while permitting cell movement during
15 tissue development.

U.S. Patent 4,352,883 describes a process for encapsulating biological materials including cells in a semipermeable spherical membrane with a predetermined porosity. Although some size and shape control is
20 possible with a membrane envelope, cell-to-cell contact, if present, is incidental and uncontrolled. U.S. Patent 4,391,909 is directed to the improvement of a semipermeable membrane envelope, similar to U.S. Patent No. 4,352,883, but with the addition of collagen within
25 the membrane envelope for cell anchorage. The semipermeable membrane in these patents is designed to prevent macromolecules and cells outside the envelope from reaching the cells enclosed within the membrane envelope. Other related patents include U.S. Patents 4,251,387,
30 4,324,683, 4,407,957, and 4,495,288. U.S. Patent 4,487,758 refines the process, teaching refinements of the older processes, optimizing water content of the hydrogel, viscosity of the alginate solution and the use of two polymer layers for forming the membrane envelope.
35 Cell-to-cell contact is again not

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promoted; the matrix is dissolved to permit the cells to float freely within the membrane enclosure. The primary object of the process and composition of the above patents is to enclose cells in a protective enveloping membrane
5 which prevents cells and macromolecules having a molecular weight averaging more than 200,000 daltons in the external environment from reaching the cells in the envelope.

It is desirable to provide
a matrix in which the individual cells are supported,
10 confined, anchored and nurtured. The matrix should be manufactured to provide any desired pore size, and in some embodiments, the matrix pores can be of such a size as to exclude cells and molecules from the external environment. In the preferred embodiments of this
15 invention, the matrix is constructed to facilitate host cellular processes such as angiogenesis and facilitate transport of macromolecules and host cells throughout the matrix.

U.S. Patent 4,353,888 also describes a process for
20 encapsulating mammalian cells within a semipermeable polymeric membrane to prevent immune rejection of the cells by antibody or immune cells of the recipient. The process involves dispersing an aqueous dispersion of the cells in a water-in-oil emulsion and coating the aqueous
25 droplets with the polymer. Shape is limited to small spheres, size control is poor, cell-to-cell contact is not effected, and no matrix is provided within the spheres.

Bell. E. et al. J. Experimental Zoology, 232:277-285
(1984) describe a process for enclosing thyroid cells in a
30 collagen matrix which contracts around the cells to produce an artificial thyroid gland for implantation. Bell et al do not achieve the cell-to-cell contact required for optimum implantation, although some

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cell-to-cell contact could be achieved if the number of cells used was sufficiently high. However, no shape, size or porosity control is possible with the Bell et al system. Other publications applying this procedure to skin grafting are Bell, E. et al. J.Invest.Dermatol. 81:2s-10s (1983); Hull, B. et al. J.Invest.Dermatol. 81:429-436 (1983); Bell, E. et al. Proc.Natl.Acad.Sci. 76:1274-1278 (1979); Hull, B. et al. J.Invest.Dermatol. 81:436-438 (1983); and U.S.Patent 4,485,096.

10 Nilsson, K. et al. Eur.J.Appl.Microbiol.Biotech. 17:319-326 (1983) describes a process for immobilizing viable cells in various monomers or polymers dispersed as a water-in-oil emulsion during matrix formation. The process yields only spherical particles and limited

15 ability to control particle size. Polymer forming materials tested by Nilsson et al include fibrin, alginates, polyacrylamides and other materials. No size or shape control is provided.

U.S.Patent 4,458,678 describes a wound healing product. Viable cells are introduced into a fibrous lattice which has some of the attributes required for an insertable matrix. However, no shape or size control is provided.

U.S.Patent 4,349,530 describes incorporating biologically active substances into cross-linked albumin particles. This process is not suitable for cells, and even if modified to accommodate cells, would not provide the cell-to-cell contact or control of size, shape or porosity required for cellular insertion.

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The cell containing matrix of this invention is prepared by

1) effecting polymerization of matrix and reversible gel precursors in an aqueous mixture f

35 a) viable cells to be incorporated into a matrix,

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- b) matrix precursor, and
 - c) reversible gel precursor
- to yield an insoluble matrix;
- 2) separating the insoluble matrix from the polymerization promoting solution;
 - 3) effecting solubilization of gel polymer in the insoluble matrix; and
 - 4) recovering an insoluble, porous matrix containing viable cells,
- wherein the solution ingredients, reagents used to effect the polymerization and/or dissolution and the temperatures are selected to maintain viability of the cells.
- Depending upon the selection of matrix precursor and reversible gel precursor, the polymerization can be effected by exposing the respective precursor to a polymerization promoting reagent and/or a polymerization promoting condition. Likewise, depending upon the nature of the reversible gel polymer, the dissolution of the gel polymer component of the matrix can be effected by choice of a suitable chemical composition or other condition of the solution in which the matrix is surrounded.

The cell containing matrix of this invention comprises viable cells incorporated into a porous matrix of a non-toxic, cell compatible polymer, the matrix having the porosity required for cell movement and the cell-to-cell contact required for growth and reorganization to permit normal functioning after insertion into the body.

The cell containing matrix intermediate of this invention comprises viable cells incorporated into a solid matrix of matrix polymer and reversible gel polymer, the cells having the cell-to-cell contact required for growth after dissolution of the reversible gel polymer.

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For a cell implant or other type of viable cell insert to be effective, the cells must undergo any reorganization, growth and differentiation which is required to permit the cells to achieve normal functioning in the body. For a three-dimensional matrix holding the cells in a unitary mass to promote this result, it preferably satisfies all of the following criteria. The process used for forming the matrix should be rapid and sufficiently gentle to prevent cellular damage. The materials used should permit a rapid reaction under these gentle conditions. The process should allow shape and size control. For a process to be generally applicable for a variety of cells, it should produce shapes having controllable final cell densities ranging from particles containing one to a few cells to shapes containing cells at a density approaching the cell density in tissue, preferably approximately from 10^9 - 10^{10} cells/cc.

The ranges of size of the particles should be selected to promote cell viability in a physiological environment. Soon after implantation, diffusion of oxygen and nutrients into the central interior of particles having excessive diameters would be insufficient, causing death of cells in the central interior. However, if the particle diameters are very small, the particles (and the cells enclosed in their matrix) may be successfully attacked by humoral or cellular components of the host immune system. Since with increasing diameters, surface areas of particles increase more slowly than enclosed volumes, larger particles would be more resistant to such attacks. Thus the particle size should be selected to balance these factors. Suitably, the particle sizes are limited to a size of from 20 to 5000 microns or preferably 20 to 3000 microns, and are most preferably within a range of from 50 to 100 microns. The optimum particle

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size is within the range of from 100 to 500 microns.

The final matrix must be nontoxic and biocompatible, and it can be biodegradable. The process should provide the ability to vary and control the matrix porosity to the
5 level necessary to permit the requisite diffusion of nutrients and macromolecules. The process should be able to provide matrices which partially immobilize the cells to encourage cell-to-cell contact while being sufficiently loose to permit cell movement which may be necessary for
10 rearrangement during tissue development. The matrix composition should also be susceptible to the degradation, removal or alteration in the host environment which is required for entry of the host cells into the matrix during the vascularization process. The process and
15 composition of this invention can satisfy these criteria wholly or in large measure.

The first step of the process of this invention may comprise contacting a first aqueous solution containing cells and polymer precursors with a second aqueous
20 polymerization promoting solution until a solid matrix of matrix polymer and reversible gel polymer containing cells is formed. The polymer precursors include a matrix precursor and a reversible gel precursor.

Matrix precursors are water-soluble compounds and
25 compositions which can be polymerized to form a solid matrix within which cells can achieve the reorganization, growth and/or differentiation required for successful adaptation. They must form a matrix structure which is sufficiently stable to substantially retain its
30 configuration after reversible gel polymer is removed to leave a porous structure. They must be non-toxic, biocompatible and can be biodegradable. They must undergo the polymerization to form the solid, insoluble structure under conditions which do not interfere with
35 polymerization of the reversible gel precursor, and must

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remain insoluble under conditions wherein the reversible gel polymer can be solubilized.

The preferred matrix precursors yield polymers which undergo spacial contraction during polymerization. These preferred matrix precursors are capable of bringing cells into closer proximity during polymerization, increasing cell-to-cell contact.

Examples of suitable matrix precursors and the reagents and/or temperature conditions effecting polymerization are listed in Table A.

TABLE A

<u>Matrix Polymer</u>	<u>Promoter</u>
Plasma Ca ⁺²	Endogenous Thrombin via Activation ^b
Fibrinogen	Thrombin ^a
Casein	Renin/pepsin ^a
Fibrin	Factor XIII(a) ^a
Limulus lysate	Endotoxin ^a
Milk protein	Renin/pepsin ^a
Collagen, all types (I, II and III)	Elevated temperature at neutral pH ^b

^a Promoter is provided in the first solution

^b Promoter is provided in a second solution

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When the matrix precursor is plasma, the matrix polymerization promoter is introduced in the second solution with the gel precursor polymerization promoter. When the matrix precursor is collagen, the polymerization
5 is effected by elevated temperature of the second solution containing the gel precursor polymerization promoter.

The reversible gel precursors must also be water-soluble, non-toxic and biocompatible. Additionally, they should rapidly polymerize or gel to form a solid
10 structure under conditions which do not interfere with the polymerization of the matrix precursor to form the matrix polymer. Furthermore, the gel polymer must be susceptible of depolymerization or dissolution under conditions which will not significantly affect the structure of the matrix
15 polymer or cell viability. The function of the gel polymer in the composition is to form an integral structure with the cells and matrix polymer which, when removed, will leave a pore structure in the matrix. The pore structure, while leaving the cells partially
20 immobilized, should allow sufficient cell movement for rearrangement during tissue development, as well as permitting diffusion of nutrients and macromolecules to and from the cells.

The gel polymer precursors are gelled by reagent
25 and/or temperature conditions in the second solution.

Examples of suitable gel precursors, the conditions and/or reagents promoting polymerization, and the agents and/or conditions effecting dissolution are listed in Table B.

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TABLE B

Gel Polymer	Promoter ^b	Dissolution
<u>Precursor</u>	<u>Promoter^b</u>	<u>Agent</u>
5 Alginate	Ca ⁺²	Citrate
Gums ^a	Ca ⁺²	Citrate
10 Agarose	Low Temp.	Temp. elevation or agarase

^a Carrageenan, agar, guar gum, gum arabic, pectins,
15 tragacanth gum, xanthan gum, etc.

^b Promoter provided in a second solution.

The aqueous solution for the matrix precursor and the
reversible gel precursor must be free from compounds which
promote polymerization of either before the shape of the
20 product is determined. It must also provide a non-toxic,
biocompatible environment for the cells.

In general, the first solution is prepared
immediately before being introduced into the second
solution, and the shape of the product is determined by
25 interactions of the reagents and/or temperature of the
second solution with the reactants in the first solution.
The gel polymer precursor rapidly polymerizes to form an
initial shape, and the matrix polymer forms later,
retaining this shape. By having the gel polymer
30 promoting conditions and/or reagents present in the second
solution, shape formation occurs immediately upon
introduction of the first solution into the second
solution.

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The first solution should be an isotonic solution with a pH which does not significantly impair cell viability during particle formation. Preferably, the solution is an isotonic saline solution or tissue culture medium of the type which is commonly used in cell and tissue cultures. Suitable isotonic saline solutions include Hank's Balanced Salt Solution and Earle's Balanced Salt Solution. Suitable tissue media include Dulbecco's Minimal Essential Medium or RPMI 1640 medium. These formulations are set forth in the following tables.

TABLE C

Earl's Balanced Salt Solution

15	<u>Components</u>	<u>Concentration, mg/liter</u>
	Inorganic salts	
	CaCl ₂ (anhydrous)	200.00
	KCl	400.00
20	MgSO ₄ (anhydrous)	97.70
	NaCl	6800.00
	NaHCO ₃	2200.00
	NaH ₂ PO ₄ ·H ₂ O	140.00
25	Other Components	
	Glucose	1000.00
	Phenol Red	10.00

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TABLE D
Hank's Balanced Salt Solution

	<u>Components</u>	<u>Concentration, mg/liter</u>
5	Inorganic salts	
	CaCl ₂ (anhydrous)	140.00
	KCl	400.00
	KH ₂ PO ₄	60.00
10	MgSO ₄ (anhydrous)	97.70
	NaCl	8000.00
	NaHCO ₃	350.00
	Na ₂ HPO ₄ (anhydrous)	48.00
15	Other Components	
	Glucose	1000.00
	Phenol Red	10.00

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TABLE E
Dulbecco's Minimal Essential Medium

	<u>Components</u>	<u>Concentration, mg/liter</u>
5	Inorganic salts	
	CaCl ₂ (anhydrous)	200.00
	Fe(NO ₃) ₃ ·9H ₂ O	0.10
	KCl	400.00
10	MgSO ₄ (anhydrous)	97.70
	NaCl	6400.00
	NaHCO ₃	3700.00
	NaH ₂ PO ₄ ·H ₂ O	125.00
	Other Components	
15	Glucose	1000.00
	Phenol Red	15.00
	Sodium pyruvate	110.00
	Amino Acids	
	L-Arginine-HCl	84.00
20	L-Cystine-2HCl	62.59
	L-Glutamine	584.00
	Glycine	30.00
	L-Histidine-HCl·H ₂ O	42.00
	L-Isoleucine	104.80
25	L-Leucine-HCl	104.80
	L-Lysine-HCl	146.50
	L-Methionine	30.00
	L-Phenylalanine	66.00
	L-Serine	42.00
30	L-Threonine	95.20
	L-Tryptophan	16.00
	L-Tyrosine	72.00
	L-Valine	93.60

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TABLE E (Cont'd)
Dulbecco's Minimal Essential Medium

	<u>Components</u>	<u>Concentration, mg/liter</u>
5	Vitamins	
	D-Calcium pantothenate	4.00
	Choline chloride	4.00
	Folic acid	4.00
10	i-Inositol	7.00
	Nicotinamide	4.00
	Pyridoxal-HCl	4.00
	Riboflavin	0.40
	Thiamine-HCl	4.00
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TABLE F
Modified RPMI 1640 Medium

	<u>Components</u>	<u>Concentration, mg/liter</u>
5	Inorganic salts	
	Ca(NO ₃) ₂ ·4H ₂ O	100.00
	KCl	400.00
	MgSO ₄ (anhydrous)	48.90
10	NaCl	6000.00
	NaHCO ₃	2000.00
	Other Components	
	Glucose	2000.00
15	Glutathione (reduced)	1.00
	Phenol Red	5.00
	Amino Acids	
	L-Arginine (free base)	200.00
20	L-Asparagine (anhydrous)	50.00
	L-Aspartic acid	20.00
	L-Cystine·2HCl	65.20
	L-Glutamic acid	20.00
	L-Glutamine	300.00
25	Glycine	10.00
	L-Histidine (free base)	15.00
	Hydroxy-L-proline	20.00
	L-Isoleucine	50.00
	L-Leucine	50.00
30	L-Lysine-HCl	40.00
	L-Methionine	15.00
	L-Phenylalanine	15.00
	L-Proline	20.00
35	L-Serine	30.00

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TABLE F (Cont'd)
Modified RPMI 1640 Medium

	<u>Components</u>	<u>Concentration, mg/liter</u>
5	Amino acids	
	L-Threonine	20.00
	L-Tryptophan	5.00
	L-Tyrosine	20.00
10	L-Valine	20.00
	Vitamins	
	p-Aminobenzoic acid	1.00
	d-Biotin	0.20
15	D-Calcium pantothenate	0.25
	Choline chloride	3.00
	Folic acid	1.00
	i-Inositol	35.00
	Nicotinamide	1.00
20	Pyridoxine-HCl	1.00
	Riboflavin	0.20
	Thiamine-HCl	1.00
	Vitamin B ₁₂	0.005

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The solution pH is suitably from 5 to 9 and is preferably from 6 to 8. The optimum pH is from 6.8 to 7.6.

The concentration of the matrix precursor and reversible gel precursor in the solution are selected to provide the desired pore structure and rigidity, and cell attachment.

The concentration of matrix precursor for most matrices can be from 1 microgram/ml to 100 mg/ml, preferably from 50 microgram/ml to 20 mg/ml and optimally

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from 0.1 mg/ml to 6 mg/ml. Other ranges may be preferred and optimum for matrices having different matrix strengths, rigidity and different cell attachment characteristics.

- 5 The reversible gel precursor concentration determines the degree of porosity. It should be selected to yield the porosity required to permit adequate flow of nutrients and macromolecules, and when necessary, to permit sufficient cell movement for reorganization. It can be
10 from 1 microgram/ml to 100 mg/ml. For low porosity compositions, it is preferably from 1 microgram/ml to 1 mg/ml, and for high porosity compositions, it is preferably from 1 to 100 mg/ml.

- 15 The term "cell" and "cells", is defined for the purposes hereof to include tissue fragments, cell clumps and single cells. The process and product of this invention is suitable for preparing a wide variety of artificial tissues or organs prepared from single cells for insertion into the body. These cells can be
20 fibroblasts, kidney cells, liver cells, thymus cells, thyroid cells, epidermal keratinocytes or cells from other tissues and organs. The process of this invention is particularly suitable for preparing artificial pancreatic endocrine tissue from pancreatic islets or islet cells for
25 implantation into the body. This process can be used with any type of cell where implantation of the cells as an artificial tissue would be beneficial.

- Insulin-dependent diabetes mellitus is a disorder resulting from lack of properly functioning pancreatic
30 islet cells which normally produce and secrete insulin in response to glucose. For implanted cells to achieve a normal function in the body and secrete insulin in response to glucose, they may need to reproduce and reorganize to form a functioning cell grouping. The
35 process and matrix of this invention is capable of

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allowing the requisite cell-to-cell contact, diffusion of nutrients and macromolecules for cell growth, and cell mobility for cellular reorganization to the functioning cell grouping required for formation of artificial organs and tissues. The optimal pancreatic islet cells for this function are substantially fibroblast-free cell preparations derived from culturing of fetal islet cells. For purposes of clarity of explanation and not by way of limitation, the invention will be described hereinafter in terms of pancreatic islet cells, it being understood that the process and matrix product is also suitable for implanting other types of cells including cells from adult tissues and organs, and that these other types of cells can be considered as alternates in the invention description.

The cell concentration in the solution determines, together with the concentration of matrix precursor, the cell density in the final matrix product. Solution cell densities can be from 10^2 to 5×10^8 cells/ml. For matrices having low cell densities, the cell concentration in the solution can be from 10^2 to 5×10^5 cells/ml, and for matrices having high cell densities, approaching the cell density of normal tissue, the cell concentration in the solution can be from 5×10^5 to 5×10^8 cells/ml.

Pancreatic islet cells suitable for incorporation into the matrix of this invention for implantation can be derived from pancreatic tissue by numerous published procedures or they can be derived from tissue, organ or cell cultures. The optimum pancreatic islet cells for implantation are believed to be fetal pancreatic proislet cells. These can be derived from the recipient species or they can be derived from a donor species which is different from the recipient species. When implanted

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into a suitable vascularized site in the body, held together with the matrix product of this invention, the cells differentiate to produce islet cells in a vascularized environment, an artificial endocrine pancreas, which responds to serum glucose by producing and secreting insulin. Procedures for preparing pancreas tissue for transplant are described by Lafferty, K. et al in Transplantation Proceedings, 14:714 (1984) and Lacy, P. et al in Ann.Rev.Immunol. 2:183 (1984).

10 The polymerization of the matrix precursor and reversible gel precursor is effected by ingredients and/or conditions of a second aqueous polymerization promotion solution with which the primary cell, matrix precursor, and gel precursor components are contacted. The
15 ingredients of this second solution must be non-toxic, biocompatible and must promote rapid polymerization of the matrix and reversible gel precursors in the primary solution.

The term "polymerization", for the purposes of this
20 application, is defined to include any reaction by which soluble precursor materials are transformed to a shape-retaining, insoluble form, including chain formation, increase in chain length, and covalent or non-covalent cross-linking.

25 Preferred polymerization promoters include multivalent ions in solution which can form a salt with the acidic gums. The optimum ion is a physiologically compatible ion such as calcium in a concentration which provides in the mixture of the first and second solution, a calcium ion
30 concentration which promotes rapid polymerization of the gel polymer precursor.

The first aqueous solution is contacted with the second aqueous solution in a manner which yields the desired solid matrix shape and size. For the production
35 of spheres, the primary solution can be dripped or blown

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under air pressure into the secondary solution, the drop size being selected to yield the desired particle size. Alternatively, the two solutions can be quickly mixed and the mixture placed in a cavity having the general configuration of the desired product. A distribution of particles can be obtained with certain gel precursors by subjecting the secondary mixture to agitation while the primary solution is rapidly poured into the secondary solution.

10 The mixture is maintained until solidification of the gel precursor occurs. For optimal control of particle size and shape, this solidification should occur very rapidly. Gel polymer formation should occur in less than 10 minutes, preferably in less than one minute and 15 optimally in less than 10 seconds. Such solidification is more or less temperature dependent, the degree of dependence varying with the characteristics of the selected gel precursor and gel polymerization promoter. The temperature dependence of solidification is preferably 20 such that rapid solidification occurs at a temperature which is compatible with cell physiology, i.e., from 0 to 50C, preferably from 4 to 45C and optimally from 6 to 37C.

Matrix precursor polymerization is initiated by contact with a matrix polymerization promoter (or 25 promoting condition), the promoter being present in either the first or second aqueous solution. Matrix polymerization should occur at a rate which does not interfere with adequate gel polymerization. The polymerization rate is dependent upon the relative 30 concentrations of matrix precursor and matrix polymerization promoter. The rate can be adjusted by adjusting the concentration of one or both concentrations. Matrix precursor polymerization should occur in from one minute to 24 hours. The optimal rate

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is determined by the physical and chemical characteristics of the particular reaction involved and the effect of the total environment during polymerization on the particular cell type being used. Preferably, the polymerization
5 should occur in from 2 minutes to 10 hours and optimally in from 5 to 200 minutes.

The matrix solids comprising polymerized matrix precursor, gelled reversible gel precursor and cells are then removed from the solution mixture. In a preferred
10 procedure, the matrix solids are then placed into a physiologically compatible solution such as described above. This solution can contain sufficient quantities of matrix polymerization promoting agents to initiate or continue the matrix polymerization if such promoting
15 agents were not present in either the first or second aqueous solution. During this phase, contraction of the matrix structure may continue, and the cells may be brought into closer proximity.

After matrix polymerization sufficient to provide a
20 matrix integrity which will retain pores after removal of the gel polymer has been achieved, the solid matrices are removed from the polymerization solution. They are preferably rinsed to remove residual solution containing the polymerization promoting agent. A suitable rinse
25 solution is an isotonic solution, isotonic saline, or tissue culture medium as described hereinabove.

The solid matrices are then placed into a gel polymer dissolution promoting solution. The gel polymer dissolution promoting solution may contain nutrients
30 required for maintaining viability of the cells and has suitable conditions, composition, or agents to reverse the polymerization reaction which produced the gel polymer. The solution should not contain any components which impair the integrity of the matrix structure or harm the
35 cells. The solution preferably contains

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nutrients which maintain the viability of the cells. For pancreatic cells, the nutrients and nutrient media described above can be used.

For removing gel polymers of the polysaccharide type other than agarose, the solution should be devoid of multivalent ions, for when the cross-linked gel structures are exposed to a solution contain monovalent ions and is relatively deficient in multivalent ions, the multivalent ions are displaced in a reversable reaction by the monovalent ions. Preferably, removal of the multivalent ions during the depolymerization treatment is achieved by the use of sequestering agents or ion exchange resins having monovalent ions such as sodium ions in the exchange sites. Movement of the solution over the matrix surfaces promotes the gel dissolution, but excess agitation which damages the matrix structure or the cells should be avoided.

The solution preferably is maintained at a temperature of from 0 to 50C and preferably from 6 to 37C during this step. The matrix treatment is continued until the desired degree of porosity has been produced, that is, until the corresponding amount of the gel polymer has been dissolved and removed from the matrix structure. The time is temperature dependent and is generally from 5 to 60 minutes for temperatures within the range of from 6 to 37C.

Agarose polymerization, being initiated by low solution temperatures, can be reversed by elevating the solution temperature. Agarose polymer dissolution temperatures can be from 37 to 65C and are preferably from 45 to 55C. Alternatively, agarose polymers can be dissolved by treatment with an agarase solution.

The final porosity of the particles after gel polymer dissolution is dependent upon the initial concentration of the gel polymer in the particle, the degree of gel

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polymer crosslinking obtained, the degree of spatial contraction occurring during matrix polymerization, the amount of matrix crosslinking or contraction occurring after gel polymer dissolution, and other variables, including processing temperatures. These variables can affect average pore diameter, pore size distribution, average pore length, and total pore numbers. In the process and composition of this invention, pore diameters can be from 5×10^{-3} to 40 microns, preferably from 2×10^{-2} to 5 microns and optimally from 0.1 to 1 microns.

The final matrix is then recovered from the solution and placed in a nutrient medium such as those described above for maintaining the viability of the cells. The nutrient medium can be further supplemented with fetal calf serum or other conventional supplements. The nutrients required for maintenance and propagation of various cells are not a part of this invention, being well established and fully within the knowledge and skill of the person skilled in the art. For example, suitable media are described in READINGS IN MAMMALIAN CELL CULTURE. Robert Pollack (editor) second edition New York: Cold Spring Harbor Laboratory (1981) and other publications.

Further processing of the matrix to preserve or to expand or multiply the cells may be desirable, depending upon the cell type and factors involved in the insertion.

The matrix product of this invention can have a particle size as low as 0.02 mm in diameter and a size as large as 3 mm. The matrix product diameter is preferably from 0.05 to 1 mm and optimally from 0.1 to 0.3 mm. The matrix can have any desired cell density. For pancreatic islet cells, the cell density can range from 10^3 to 5×10^8 cells/cc of matrix.

The matrix is porous and has a pore size sufficiently large to permit diffusion of nutrients and macromolecules

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to and from the cells entrapped in the matrix, and movement of cells.

The matrices of this invention can be implanted in the same manner as implantation of the corresponding tissue.

5 For effective vascularization of the implanted matrix, the matrix is preferably implanted in a portion of the body which is not functionally affected by the implant and which will readily vascularize the implant. For example, if the matrix supports pancreatic islet cells, the matrix
10 can be implanted in the mesenteric omentum, kidney subcapsular space, splenic pulp, portal vein, and other sites appropriate for vascularization and function.

This invention is further illustrated by the following specific, but non-limiting examples. Unless otherwise
15 specified, temperatures are given in degrees centigrade and concentrations are given as weight percents.

EXAMPLE 1

Monolayers of cultured pancreatic pre-islet cells were harvested by trypsinization and washed twice in isotonic,
20 neutral pH buffer. The number of cells and percent viability were determined by trypan blue exclusion with a hemocytometer. Approximately 4×10^6 viable cells were recovered. The cells were maintained on ice and centrifuged (150 x g) for 5 min before use. After removal
25 of the supernatant, the cell pellet was recentrifuged (200 x g) for 1 min to facilitate removal of residual interstitial liquid.

The following components (maintained on ice) were added to an isotonic saline solution in a separate 3 ml
30 conical vial to give the component concentrations noted:

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	<u>Component</u>	<u>Concentration</u>
	Sodium alginate	1.0 %
	Collagen, Type I	0.05 mg/ml
	Collagen, Type IV	0.05 mg/ml
5	Fibronectin	0.025 mg/ml
	Laminin	0.025 mg/ml

The solution was gently mixed and used to resuspend the cell pellet at 1×10^7 cells/ml. To this suspension
10 were added fibrinogen (0.6 mg/ml final concentration) and thrombin (0.2 units/ml) to clot the fibrinogen. This final reaction mixture was rapidly aspirated into a syringe and expressed through the droplet-forming device as described in BIOMEDICAL APPLICATIONS OF
15 MICROENCAPSULATION. F. Lim (editor) Boca Raton: CRC Press (1983) at a rate of 10 ml/hr. The air flow was set at a flowmeter reading of 50 psig. Droplets were delivered into 102 mM isotonic CaCl_2 for 2-10 min until the insoluble matrix formed. A series of washes in isotonic
20 saline to remove Ca^{+2} ions and/or free alginate were preformed, and the resulting particles were resuspended in RPMI 1640 containing 10% (v/v) fetal calf serum.

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CLAIMS

1. A process for making a transplantable artificial tissue matrix comprising
 - 5 a) polymerizing polymer precursors in an aqueous solution containing a matrix polymer precursor, a reversible gel polymer precursor, and viable cells to form a shape retaining solid matrix comprising viable cells, matrix polymer and reversible gel polymer,
 - 10 b) dissolving and removing gel polymer from the matrix, and
 - c) recovering an insoluble, porous matrix containing viable cells,
- 15 wherein the condition and reagents are selected to not significantly impair the viability of the cells.
2. A process of claim 1 wherein the matrix polymer precursor is selected from plasma, fibrinogen, casein, fibrin,
- 20 limulus lysate, milk protein and collagen.
3. A process of claim 2 wherein the matrix polymer precursor is plasma, and the matrix polymer polymerization is effected by mixing the plasma with Ca^{+2} ions.
- 25 4. A process of claim 2 wherein the matrix polymer precursor is fibrinogen and the polymerization is effected by mixing the fibrinogen with thrombin.
- 30 5. A process of claim 2 wherein the matrix polymer precursor is casein or milk protein and the polymerization is effected by mixing the matrix polymer precursor with renin or pepsin.
- 35 6. A process of claim 2 wherein the matrix polymer precursor

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sor is fibrin and the polymerization is effected by mixing the fibrin with Factor XIIIa.

7. A process of claim 2 wherein the matrix polymer precursor is collagen and the polymerization is effected by raising the temperature of the collagen solution from 37 to 55°C while maintaining a neutral solution pH.

8. A process of any one of the preceding claims wherein the reversible gel polymer precursor is a polysaccharide.

9. A process of claim 8 wherein the reversible gel polymer precursor is an alginate or a polysaccharide gum, and the polymerization of the reversible gel polymer precursor is effected by mixing the reversible gel polymer precursor with Ca^{+2} ions.

10. A process of claim 9 wherein the gel polymer in the matrix is dissolved by reducing the concentration of Ca^{+2} ions in an aqueous solution containing the matrix by mixing the solution with a sequestering agent or cation exchange resin capable of binding Ca^{+2} ions, to depolymerize the gel polymer.

11. A process of claim 8 wherein the reversible gel polymer precursor is agarose, and the polymerization is effected by decreasing the temperature of the agarose solution to a level which promotes agarose polymerization.

12. A process of claim 11 wherein the reversible gel polymer in the matrix is dissolved by elevating the temperature of an aqueous solution containing the matrix to a level which promotes agarose depolymerization.

13. A process of claim 11 wherein the reversible gel polymer

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mer in the matrix is dissolved by mixing an aqueous solution containing the matrix with agarase.

14. A process of claim 8 wherein the polysaccharide is
5 selected from agarose, carrageenan, agar, alginate, guar gum, gum arabic, pectin, tragacanth gum, xanthan gum and mixtures thereof.

15. A process for making a transplantable artificial tissue
10 matrix comprising

- a) polymerizing polymer precursors in an aqueous solution containing a matrix polymer precursor, a reversible gel polymer precursor, and viable cells to form a shape retaining solid matrix comprising
15 viable cells, matrix polymer and reversible gel polymer,
 - i) wherein the matrix polymer precursor is selected from plasma, fibrinogen, casein, fibrin, limulus lysate, milk protein and
20 collagen and mixtures thereof, and
 - ii) the polysaccharide is selected from agarose, carrageenan, agar, alginate, guar gum, gum arabic, pectin, tragacanth gum, xanthan gum and mixtures thereof,
 - 25 b) dissolving and removing gel polymer from the matrix by exposing the matrix to a solution having characteristics which effect depolymerization of the gel polymer, and
 - c) recovering an insoluble, porous matrix containing
30 viable cells,
- wherein the conditions and reagents are selected to not significantly impair the viability of the cells.

16. A matrix composition comprising viable cells incorpor-
35 ated throughout a porous matrix of nontoxic biocompatible

polymer, the matrix having a particle size of from 0.02 to 5 mm and a pore structure and size permitting cell movement within the matrix and movement of host cells into the matrix and diffusion of nutrients and macromolecules into and out
5 of the matrix.

17. A matrix composition of claim 16 wherein the matrix is a product of the polymerization of a matrix polymer precursor selected from plasma, fibrinogen, casein, fibrin,
10 limulus lysate, milk protein and collagen and mixtures thereof.

18. A matrix composition of claim 16 or claim 17 wherein the viable cells are pancreatic islet cells.
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19. A matrix composition produced by the process of any one of claims 1 to 15.

20. A matrix composition of claim 19 wherein the viable
20 cells are pancreatic islet cells.